

ARTIFICIAL INTERVERTEBRAL DISC HAVING A BORED SEMISPHERICAL BEARING WITH A COMPRESSION LOCKING POST AND RETAINING CAPS

FIELD OF THE INVENTION

5 [0001] This invention relates generally to a device for implantation into an intervertebral space to simultaneously stabilize the adjacent vertebral bodies and permit proper anatomical motion at the segment. Specifically, the present invention relates to such a device having upper and lower baseplates that articulate about a central, bored semispherical bearing. The present invention maximizes the strength (i.e., compression
10 and tension load capabilities) of such a device by allowing the semispherical bearing to have a larger diameter without increasing the height of the device.

BACKGROUND OF THE INVENTION

 [0002] The bones and connective tissue of an adult human spinal column consist
15 of more than twenty discrete bones coupled sequentially to one another by a tri-joint complex, which consists of an anterior disc and two posterior facet joints, the anterior discs of adjacent bones being cushioned by cartilage spacers referred to as intervertebral discs. These more than twenty bones are anatomically categorized as being members of one of four classifications: cervical, thoracic, lumbar, or sacral. The cervical portion of the
20 spine, which comprises the top of the spine up to the base of the skull, includes the first seven vertebrae. The intermediate twelve bones are the thoracic vertebrae, and connect to the lower spine comprising the five lumbar vertebrae. The base of the spine comprises the sacral bones (including the coccyx). The component bones of the cervical spine are generally smaller than those of the thoracic spine, which are in turn smaller than those
25 of the lumbar region. The sacral region connects laterally to the pelvis.

[0003] The spinal column is highly complex in that it includes these more than twenty bones coupled to one another, housing and protecting critical elements of the nervous system having innumerable peripheral nerves and circulatory bodies in close proximity. In spite of these complications, the spine is a highly flexible structure, capable
5 of a high degree of curvature and twist in nearly every direction.

[0004] Genetic or developmental irregularities, trauma, chronic stress, tumors, and degenerative wear are a few of the causes that can result in spinal pathologies for which surgical intervention may be necessary. A variety of systems have been disclosed in the art that achieve immobilization and/or fusion of adjacent bones by implanting
10 artificial assemblies in or on the spinal column. The region of the back that needs to be immobilized, as well as the individual variations in anatomy, determine the appropriate surgical protocol and implantation assembly. With respect to the failure of the intervertebral disc, the interbody fusion cage has generated substantial interest because it can be implanted laparoscopically into the anterior of the spine, thus reducing
15 operating room time, patient recovery time, and scarification.

[0005] Referring now to **Figs. 2-3**, in which a side perspective view of an intervertebral body cage and an anterior perspective view of a post implantation spinal column are shown, respectively, a more complete description of these devices of the prior art is herein provided. These cages **1** generally comprise tubular metal body **2**
20 having an external surface threading **3**. They are inserted transverse to the axis of the spine **4**, into preformed cylindrical holes at the junction of adjacent vertebral bodies (in **Fig. 3** the pair of cages **1** are inserted between the fifth lumbar vertebra (L5) and the top of the sacrum (S1)). Two cages **1** are generally inserted side by side with the external surface threading **3** tapping into the lower surface of the vertebral bone above (L5), and

the upper surface of the vertebral bone (S1) below. The cages 1 include holes 5 through which the adjacent bones are to grow. Additional materials, for example autogenous bone graft materials, may be inserted into the hollow interior 6 of the cage 1 to incite or accelerate the growth of the bone into the cage. End caps (not shown) are often utilized
5 to hold the bone graft material within the cage 1.

[0006] These cages of the prior art have enjoyed medical success in promoting fusion and grossly approximating proper disc height. It is, however, important to note that the fusion of the adjacent bones is an incomplete solution to the underlying pathology as it does not cure the ailment, but rather simply masks the pathology under
10 a stabilizing bridge of bone. This bone fusion limits the overall flexibility of the spinal column and artificially constrains the normal motion of the patient. This constraint can cause collateral injury to the patient's spine as additional stresses of motion, normally borne by the now-fused joint, are transferred onto the nearby facet joints and intervertebral discs. It would therefore, be a considerable advance in the art to provide
15 an implant assembly which does not promote fusion, but, rather, which mimics the biomechanical action of the natural disc cartilage, thereby permitting continued normal motion and stress distribution.

[0007] It is, therefore, an object of the invention to provide an intervertebral spacer that stabilizes the spine without promoting a bone fusion across the intervertebral
20 space.

[0008] It is further an object of the invention to provide an implant device that stabilizes the spine while still permitting normal motion.

[0009]

It is further an object of the invention to provide a device for implantation into the intervertebral space that does not promote the abnormal distribution of biomechanical stresses on the patient's spine.

[0010] It is further an object of the invention to provide an artificial
5 intervertebral disc that supports compression loads.

[0011] It is further an object of the invention to provide an artificial intervertebral disc that supports tension loads.

[0012] It is further an object of the invention to provide an artificial intervertebral disc that prevents lateral translation of the baseplates relative to one
10 another.

[0013] It is further an object of the invention to provide an artificial intervertebral disc that provides a centroid of motion centrally located within the intervertebral space.

[0014] It is further an object of the invention to provide artificial intervertebral
15 disc that provides maximized strength without increasing the height of the disc.

[0015] Other objects of the invention not explicitly stated will be set forth and will be more clearly understood in conjunction with the descriptions of the preferred embodiments disclosed hereafter.

20 SUMMARY OF THE INVENTION

[0016] The preceding objects are achieved by the invention, which is an artificial intervertebral disc or intervertebral spacer device, comprising a pair of support members (e.g., spaced apart baseplates), each with an outwardly facing surface. Because the artificial disc is to be positioned between the facing endplates of adjacent vertebral

bodies, the baseplates are arranged in a substantially parallel planar alignment (or slightly offset relative to one another in accordance with proper lordotic angulation) with the outwardly facing surfaces directed away from one another. The baseplates are to mate with the vertebral bodies so as to not rotate relative thereto, but rather to permit the spinal segments to bend or axially compress relative to one another in manners that mimic the natural motion of the spinal segment. This natural motion is permitted by the performance of a bearing disposed between the secured baseplates, and the securing of the baseplates to the vertebral bone is preferably achieved through the use of a vertebral body contact element attached to, or a surface feature of, the outwardly facing surface of each baseplate.

[0017] Preferable body contact elements include, but are not limited to, a convex mesh (of any shape or contour, but preferably domed) and one or more spikes. These vertebral body contact elements are disclosed in greater detail in Application Serial No. 10/256,160 ("the '160 Application") and Application Serial No. 10/642,258 ("the '258 Application"), which are incorporated herein by reference.

[0018] To enhance the securing of the baseplates to the vertebral bones, each baseplate preferably further comprises a surface feature that permits the long-term ingrowth of vertebral bone into the baseplates. A preferred surface feature is a porous area, which at least extends in a ring around the lateral rim of each outwardly facing surface. The porous area may be, for example, a sprayed deposition layer, an adhesive applied beaded metal layer, or another suitable porous coating known in the art. The porous ring permits the long-term ingrowth of vertebral bone into the baseplates, thus permanently securing the prosthesis within the intervertebral space.

[0019] The semispherical bearing disposed between the baseplates permits rotation and angulation of the two baseplates relative to one another and to the bearing, which establishes a centroid of motion (for this rotation and angulation) centrally between the baseplates. The semispherical bearing is captured between the baseplates by first and second retaining caps which are connected together by engagement of compression locking posts. Further, the capturing prevents separation and/or disassembly of the device under tension loading, and prevents lateral translation of the baseplates, during the rotation and angulation.

[0020] More specifically, the two baseplates of the present invention each include an aperture and each is secured to a bored central bearing in the following manner. The first and second baseplates are disposed such that their outwardly facing surfaces face away from one another, and their inwardly facing surfaces are directed toward one another. The second baseplate aperture is then passed over the compression locking post of second retaining cap and integral second retaining cap such that the compression locking post passes through the outwardly facing surface first and the inwardly facing surface second. A circumferential protrusion in the second baseplate aperture wall (i.e., the axially inwardly directed surface of the second baseplate) will rest upon the inwardly facing surface of the second retaining cap. Next, the bore of the central bearing is passed over the compression locking post and into the second baseplate aperture until a portion of the bearing having a smaller diameter contacts the inwardly facing surface of the second retaining cap and a portion of the bearing having a larger diameter contacts the inwardly facing surface of the circumferential protrusion in the wall of the second baseplate aperture. Then, the first baseplate aperture is passed over the compression locking post until the circumferential protrusion in the first

baseplate aperture wall (i.e., the axially inwardly directed surface of the first baseplate) rests upon the bearing. Finally, compression locking post of the first retaining cap is pressed into the bearing bore and over the compression locking post of the second retaining cap under a force sufficient to compression lock the two compression locking posts, its integral retaining caps, and the bearing. At this point, the two retaining caps, compression locking posts, and bearing become one stationary unit (i.e., the retaining caps, compression locking posts, and bearing do not rotate or otherwise move relative to each other). The baseplates are free to rotate and articulate about the bearing and its firmly affixed retaining caps and post).

[0021] After assembly, as described above, the inwardly facing surfaces of the baseplate aperture walls (i.e., the surfaces extending from the circumferential protrusion in each aperture wall to the inward edge of each aperture wall) provide bearing surfaces, within which the bearing is captured, thereby facilitating limited angulation of the baseplates relative to the bearing. These bearing surfaces are preferably contoured to closely accommodate the spherical contour defined by the bearing, such that the bearing may easily contact and slide against the bearing surfaces. In this manner, the baseplate bearing surfaces, and therefore the baseplates, may angulate with limitation about the bearing.

[0022] As noted above, angulation of the baseplates relative to the bearing is limited. The outwardly facing surfaces of the baseplate aperture walls (i.e., the surfaces extending from the circumferential protrusion in each aperture wall to the outward edge of each aperture wall) are tapered to a larger diameter toward the baseplate's outwardly facing surfaces. Additionally, and preferably, the conformation of the taper matches the contour defined by the inwardly facing surface of the respective retaining cap. Because

the retaining caps and posts are stationary with respect to the bearing, such tapering and conformation of the baseplate aperture wall permits the baseplates to angulate (about the centroid of motion at the center of the bearing) with respect to the bearing until the point at which the baseplate interferes with, or contacts, the respective retaining cap.

5 Therefore, the taper, diameter, and conformation of this articulation (i.e., the space between the retaining cap and its respective baseplate) limit the angular movement of the respective baseplate relative to the bearing. Preferably, the taper, diameter, and conformation of the taper accommodate rotation of the respective baseplate relative to the bearing at least until the inwardly facing surfaces of the baseplates meet.

10 [0023] Furthermore, in the preferred embodiment of the present invention, the axial rotation of each baseplate is limited, preferably to between 7 and 10 degrees. This limitation may be created using a variety of methods. For example, this can be realized by a notch and groove, wherein notches are formed in each retaining cap and grooves are formed in each baseplate. Alternatively, the grooves may be formed in the retaining
15 caps and the notches may be formed in the baseplates.

[0024] Accordingly, the baseplates rotate with limitation relative to the bearing. Because the bearing is secured to the baseplates with the compression locking posts and retaining caps as discussed above, the artificial intervertebral disc of the present invention can withstand tension loading of the baseplates, and the assembly does not
20 come apart under normally experienced tension loads. Thus, in combination with the securing of the baseplates to the adjacent vertebral bones, the disc assembly has an integrity similar to the tension-bearing integrity of a healthy natural intervertebral disc. Also because the bearing is laterally captured between the bearing surfaces, lateral translation of the baseplates relative to one another is prevented during rotation and

angulation, similar to the performance of a healthy natural intervertebral disc. The baseplates are designed to rotate relative to the bearing, therefore, the disc assembly provides a centroid of motion within the bearing. Accordingly, the centroid of motion of the disc assembly remains centrally located between the vertebral bodies, similar to the
5 centroid of motion in a healthy natural intervertebral disc.

[0025] In addition to the features and functions described above for the baseplate apertures, the present invention can take advantage of the concavities of the adjacent vertebral bodies, and allow the size of the bearing, and accordingly its ability to withstand compression and tension loads, to be maximized. Specifically, the present
10 invention is designed to allow each retaining cap to protrude beyond the outwardly facing surface of the respective baseplate into the concavity of the vertebral body adjacent to the outwardly facing surface, facilitating rotation of the baseplate on the bearing 28. Moreover, enlargement of the bearing creates a more robust bearing assembly that is able to withstand greater compression and tension forces than the same
15 bearing assembly having a smaller size.

[0026] It should be understood that each of the features of the preferred and alternate embodiments described herein, including, but not limited to, formations and functions of baseplates, manners of contacting the bearing ball with bearing surfaces, manners of limiting rotation of the baseplates relative to one another, and manners of
20 allowing the bearing mechanism to extend into the concavities of adjacent vertebral bodies, can be included in other embodiments, individually or with one or more of the other features, in other permutations of the features, including permutations that are not specifically described herein, without departing from the scope of the present invention.

BRIEF DESCRIPTION OF THE DRAWINGS

[0027] FIGS. 1a-c show top (FIG. 1a), side (FIG. 1b), and bottom (FIG. 1c) views of an assembled preferred embodiment of the present invention.

[0028] FIGS. 1d - 1e show exploded (FIG. 1d) and assembled (FIG. 1e) views of
5 the preferred embodiment of the present invention.

[0029] FIGS. 1f - 1h show side cutaway perspective exploded (FIG. 1f) and side cutaway assembled perspective and straight (FIGS. 1g and 1h) views of the preferred embodiment of the present invention.

[0030] FIG. 2 shows a side perspective view of a prior art interbody fusion
10 device.

[0031] FIG. 3 shows a front view of the anterior portion of the lumbo-sacral region of a human spine, into which a pair of interbody fusion devices (as shown in FIG. 2) have been implanted.

15 DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

[0032] While the invention will be described more fully hereinafter with reference to the accompanying drawings, in which particular embodiments and methods of implantation are shown, it is to be understood at the outset that persons skilled in the art may modify the invention herein described while achieving the
20 functions and results of the invention. Accordingly, the descriptions that follow are intended to be illustrative and exemplary of specific structures, aspects, and features within the broad scope of the invention and not as limiting of such broad scope.

[0033] Referring first to FIGS. 1g and 1h, the artificial intervertebral disc assembly of the present invention generally comprises first and second endplates 10, 30

rotatably retained on a bearing 28 of a bearing mechanism which comprises bearing 28 and first and second retaining caps 12, 34. When assembled as shown in FIGS. 1g and 1h, retaining caps 12, 34 are connected to each other by engagement of respective compression locking posts 64, 14, whereby retaining caps 12, 34 and bearing 28 form an integrated piece and cannot move relative to one another, which will be explained in greater detail.

[0034] Referring also to FIGS. 1a-c, the assembled artificial intervertebral disc of the present invention is shown in top (FIG. 1a), side (FIG. 1b), and bottom (FIG. 1c) views. Generally, first baseplate 10 and second baseplate 30 rotate relative to bearing 28, which is captured between baseplates 10, 30 via first retaining cap 12 and second retaining cap 34. This capturing is accomplished by a compression locking post 14 of second retaining cap 34 and a compression locking post 64 of first retaining cap 12 compression locking to one another (via a bore 38 in compression locking post 64) and into axial bores 56, 60 in bearing 28 (See also FIGS. 1d-h.).

[0035] More specifically, FIG. 1a depicts a top view of first baseplate 10, first retaining cap 12, compression locking post 14, first baseplate beveled edges 16, and first baseplate aperture 18 of the preferred embodiment of the present invention.

[0036] First baseplate 10, as well as second baseplate 30 (FIGS. 1b-c), are solid baseplates preferably comprised of a metal or metal alloy, such as a metal alloy including cobalt-chromium. However, baseplates 10, 30 may also be comprised of other types of metal or non-metal materials without departing from the scope of the present invention.

[0037] As shown in FIG. 1d, compression locking post 64 of first retaining cap 12 has a compression locking post aperture 38 (FIG. 1d) slightly smaller in diameter than

the outer diameter of compression locking post 14. This dimensional difference allows compression locking post 14 to be attached to compression locking post 64 of first retaining cap 12 via a compression lock (i.e., forcing compression locking post 14 into compression locking post 64 of first retaining cap aperture 38 via application of pressure, such that the two cannot be separated absent a separation force greater than those experienced under spinal loads that can be survived by the patient). Alternatively or in addition to a compression locking attachment method, other methods of attaching compression locking post 14 to compression locking post 64 of first retaining cap 12 may be incorporated, including, but not limited to, laser welding (i.e., the laser weld may be applied from the outwardly facing surface of compression locking post 64 of first retaining cap 12 at the point where it contacts compression locking post 14), threading, etc. Thus, first and second retaining caps 12, 34 and bearing 28 sandwiched therebetween form an integrated piece and cannot move relative to one another. The integration of caps 12, 34 and bearing 28 can also be realized or enhanced by compression locking (or threading engagement, etc) between posts 14, 64 and bearing bores 60, 56.

[0038] Referring to FIGS. 1d and 1f, first baseplate 10 includes first baseplate outwardly facing surface 22 and first baseplate aperture 18. The aperture wall (i.e., the axially inwardly directed surface) of first baseplate 10 contains a first baseplate circumferential protrusion 40 (FIG. 1f) that retains first baseplate 10 between first retaining cap 12 and bearing 28 while allowing first baseplate 10 to rotate relative to bearing 28, as described in greater detail below with respect to FIG. 1f.

[0039] Referring next to FIG. 1b, shown is a side view of baseplates 10, 30 and bearing 28. Also depicted in FIG. 1b, first baseplate inwardly facing surface 20 is flat,

and first baseplate outwardly facing surface **22** is shaped as a convex dome. Similarly, second baseplate inwardly facing surface **24** is flat, and second baseplate outwardly facing surface **26** is shaped as a convex dome. Although the outwardly facing surfaces **22, 26** of baseplates **10,30** of the preferred embodiment of the present invention are preferably shaped as convex domes so as to match the shape of the endplates of adjacent vertebral bodies to which the baseplates **10, 30** are to be attached, it should be noted that the outwardly facing surfaces of the baseplates are not limited to this particular shape. Also, as depicted, because clearance between retaining caps **12, 34** and baseplates **10, 30** allows rotation of the baseplate on the bearing **28**, retaining caps **12, 34** may protrude slightly from baseplate outwardly facing surfaces **22, 26** during such rotation. After insertion of the device between vertebral bodies, retaining caps **12, 34** protrude slightly into the concavities of vertebral bodies located adjacent to baseplates **10, 30**, respectively.

[0040] Since the artificial disc of the present invention is to be positioned between the facing surfaces of adjacent vertebral bodies, baseplates **10, 30** of the present invention are disposed such that baseplate outwardly facing surfaces **22, 26** face away from one another as best illustrated in the assembly view in **FIG. 1d**. Baseplate outwardly facing surfaces **22, 26** include first baseplate beveled edges **16 (FIG. 1a)** and second baseplate beveled edges **36 (FIG. 1c)**, respectively, and are designed to conform to the overall shape of the respective endplates of the vertebral bodies with which they will mate.

[0041] Preferably, baseplate outwardly facing perimeter regions **17, 33 (FIGS. 1a, 1c)** of baseplate outwardly facing surfaces **22, 26** are osteoconductive due to, for example, a sprayed deposition layer, an adhesive applied beaded metal layer, or a similar suitable porous coating that is applied to these surfaces using methods known in

the art. These baseplate outwardly facing surfaces 22, 26 permit the long-term ingrowth of vertebral bone into baseplates 10, 30, thus permanently securing the artificial intervertebral disc within the intervertebral space. The material applied to create the osteoconductive baseplate outwardly facing perimeter regions 17, 33 of baseplate
5 outwardly facing surfaces 22, 26 may extend closer to baseplate apertures 18, 32. However, it is most important that this osteoconductive material is applied to the portions of baseplate outwardly facing surfaces 22, 26 that seat directly against the adjacent vertebral body.

[0042] An alternate embodiment of the present invention may include one or
10 more vertebral body contact elements including, but not limited to, a convex mesh, a convex dome, and one or more spikes as disclosed in the '160 and '258 Applications. These elements could be attached to baseplate outwardly facing surfaces 22, 26, also as described in the '160 and '258 Applications.

[0043] It should also be noted that depending upon the magnitude of expansion
15 or contraction of the baseplates relative to each other, if any, first retaining cap 12 and second retaining cap 34, might protrude outward from the baseplate outwardly facing surfaces 22, 26, respectively. It should be further noted that the convex mesh, also disclosed in the '160 Application, is suitable for use with the present invention, and preferably should be attached to baseplate outwardly facing surfaces 22, 26, outside of
20 the area of motion of retaining caps 12, 34. Such attachment may be performed via a variety of methods including, but not limited to laser welding, or more preferably, plasma burying (i.e., the perimeter region of the convex mesh is buried under a plasma coating, which coating secures to the outwardly facing surface of the baseplate to which it is applied, and thus secures the convex mesh to the outwardly facing surface).

Preferably, the convex mesh has a concavity such that contact with retaining caps 12, 34 is avoided.

[0044] Baseplates 10, 30 are designed to mate with the vertebral bodies such that they do not rotate relative thereto, but rather permit the spinal segments to bend relative to one another in manners that mimic the natural motion of the spinal segment. This motion is permitted by the performance of bearing 28 disposed between baseplates 10, 30, which are secured thereto via compression locking posts 14, 64 (FIG. 1d), first retaining cap 12 (FIG. 1a), and second retaining cap 34 (FIG. 1c).

[0045] Baseplates 10, 30 are joined with bearing 28, first retaining cap 12, and second retaining cap 34. In a preferred embodiment of the present invention, bearing 28 has a semispherical shape, however, other shapes may be incorporated without departing from the scope of the present invention. Each of baseplates 10, 30 includes bearing surfaces 70, 74 (FIG. 1f), respectively, within which bearing 28 is capturable to allow limited rotation of baseplates 10, 30 relative to bearing 28. Each bearing surface is semispherically contoured to closely accommodate and engage with the spherical contour defined by bearing 28, such that baseplates 10, 30 may rotate transverse to the axis of the spine and may rotate relative to bearing 28 about a centroid of motion located at the center of bearing 28. As illustrated in FIG. 1f, bearing 28 includes first bearing bore 56, which accepts compression locking post 64 protruding from first retaining cap 12 (FIG. 1d), as well as second bearing bore 60, which accepts compression locking post 14 inserted into compression locking post aperture 38 of compression locking post 64. Preferably, compression locking post 64 locks into first bearing bore 56 via a compression lock. In the preferred embodiment of the present invention, the bearing bore comprises a first bearing bore 56 and a second bearing bore 60, each section having

a different diameter, however, an alternate embodiment of the present invention may include a single bearing bore having a single, consistent diameter.

[0046] In the preferred embodiment of the present invention, the diameter of bearing 28 is slightly larger than the diameters of baseplate apertures 18, 32 (FIG. 1a, 1c), such that during axial compression of baseplates 10, 30 and no, or minimal, angular rotation of either of baseplates 10, 30, baseplate bearing surfaces 70, 74 directly contact axially outwardly directed bearing surface 48, and baseplate inwardly facing surfaces 20, 24 do not make contact. Therefore, in an axially compressed state, baseplates 10, 30, and the vertebral bodies adjacent thereto, retain the ability to rotate relative to bearing 28.

This allowed rotation mimics that found in the corresponding sections of a natural spine.

[0047] Referring next to FIG. 1c, shown are bottom views of second baseplate 30, second baseplate aperture 32, second baseplate outwardly facing perimeter region 33, second retaining cap 34, and second baseplate beveled edges 36. In the preferred embodiment of the present invention, second retaining cap 34 and compression locking post 14 (FIG. 1a) are manufactured as a single component. However, in an alternate embodiment of the present invention, second retaining cap 34 and compression locking post 14 are manufactured as separate components and are affixed to each other during assembly of the present invention. The methods of attachment include, but are not limited to, compression locking and threading.

[0048] Turning next to FIGS. 1d and 1e, shown are an exploded view (FIG. 1d) and an assembly view (FIG. 1e) of the preferred embodiment of the present invention. Assembly of the artificial intervertebral disc is as follows. Baseplates 10, 30 are disposed such that their baseplate outwardly facing surfaces 22, 26, respectively, face away from

one another and their baseplate inwardly facing surfaces 20, 24, respectively, are directed toward one another. Second baseplate aperture 32 is then passed over compression locking post 14 and integral second retaining cap 34 such that compression locking post 14 passes through second baseplate outwardly facing surface 26 first and
5 through second baseplate inwardly facing surface 24 second, and until the second retaining cap inwardly facing tapered surface 80 is in contact with tapered second baseplate outwardly facing aperture wall surface 76 (FIG. 1f) (i.e., the surface extending from second baseplate circumferential protrusion 46 (FIG. 1f) to the outward edge of the aperture wall). Next, second bearing bore 60 (FIG. 1f), and, consequently, first bearing
10 bore 56 (FIG. 1f), are passed over compression locking post 14 until outwardly facing bearing surface 50 contacts inwardly facing second retaining cap surface 52 of second retaining cap 34 and axially outwardly directed bearing surface 48 contacts second baseplate bearing surface 74 (FIG. 1f). Then, first baseplate aperture 18 is passed over compression locking post 14 until first baseplate circumferential protrusion 40 (FIG. 1f)
15 and first baseplate bearing surface 70 contact axially outwardly directed bearing surface 48. Finally, **compression locking post 64 of first retaining cap 12** is passed over compression locking post 14 into first bearing bore 56 (FIG. 1f) under a force sufficient to radially compress compression locking post 14 and radially expand first bearing bore 56 (FIG. 1f). Force is applied until inwardly facing first retaining cap surface 54 is in
20 contact with second bearing bore inwardly facing surface 58 (FIG. 1f) of second bearing bore 60 (FIG. 1f). After the force is removed, the radial pressure exerted by compression locking post 14 on first retaining cap axially inwardly directed surface (inner surface) 62 (FIG. 1f) of compression locking post 64 of first retaining cap 12, as well as the radial pressure exerted by **compression locking post 64** on first bearing bore 56 (FIG. 1f), acts

to lock first retaining cap 12, bearing 28, and second retaining cap 34, such that these components do not separate and do not rotate or, otherwise move, relative to each other.

[0049] Referring next to FIGS. 1f - 1h, shown are a side cutaway exploded view (FIG. 1f) and a side cutaway assembly view (FIGS. 1g and 1h) of the preferred
5 embodiment of the present invention. These side cutaway views depict the internal dimensions of each of the components of the present invention as well as the assembled configuration of each component relative to the other components.

[0050] As depicted in FIG. 1f, first retaining cap 12 comprises outward first retaining cap section 66, first retaining cap inwardly facing tapered surface 68, and
10 compression locking post 64, which has a smaller diameter than outward first retaining cap section 66 [see above]. Similarly, first baseplate 10 has first baseplate circumferential protrusion 40, having the smallest diameter of any portion of first baseplate 10, and tapered first baseplate outwardly facing aperture wall surface 72, which is tapered to mate with first retaining cap inwardly facing tapered surface 68. Furthermore, first
15 baseplate 10 has a first baseplate bearing surface 70 having a concavity equivalent, or near equivalent, to the contour defined by bearing 28.

[0051] Similarly, also as depicted in FIG. 1f, compression locking post 14 with integral second retaining cap 34 comprises outward second retaining cap section 78 and second retaining cap inwardly facing tapered surface 80. Second baseplate 30 has a
20 second baseplate circumferential protrusion 46 having the smallest diameter of any portion of second baseplate 30, and tapered second baseplate outwardly facing aperture wall surface 76 tapered to mate with second retaining cap inwardly facing tapered surface 80. Furthermore, second baseplate 30 has a second baseplate bearing surface 74 having a concavity equivalent, or near equivalent, to the contour defined by bearing 28.

[0052] Accordingly, due to these configurations, the baseplates 10, 30 are able to rotate relative to bearing 28. The semispherical contour of first baseplate bearing surface 70 closely matches the spherical contour defined by bearing 28, such that first baseplate 10 can rotate about the centroid of motion located at the center of bearing 28. Further, tapered first baseplate outwardly facing aperture wall surface 72 is tapered to a larger diameter toward the first baseplate outwardly facing surface 22. Additionally, and preferably, the conformation of the taper matches the contour defined by first retaining cap inwardly facing tapered surface 68. Since first retaining cap 12 and compression locking post 64 are stationary with respect to bearing 28, such tapering and conformation of tapered first baseplate outwardly facing aperture wall surface 72 permits first baseplate 10 to rotate (about the centroid of motion at the center of bearing 28) with respect to bearing 28 until the point at which first baseplate 10 interferes with, or contacts, the first retaining cap inwardly facing tapered surface 68. Therefore, the taper, diameter, and conformation of these interacting elements (i.e., the formation of the space between first retaining cap 12 and first baseplate 10) can be established to limit the rotational ability of the first baseplate 10 relative to bearing 28. Preferably, the taper, diameter, and conformation of these interacting elements accommodate rotation of first baseplate 10 relative to bearing 28 at least until baseplate inwardly facing surfaces 20, 24 of baseplates 10, 30 meet. In other words, the ability of first baseplate 10 to rotate relative to bearing 28 is limited by the distance between first retaining cap inwardly facing tapered surface 68 and first baseplate 10, as well as the distance between baseplates 10, 30.

[0053] Similarly, the semispherical contour of second baseplate bearing surface 74 closely matches the spherical contour defined by bearing 28, such that bearing 28 can

rotate about the about a centroid of motion located at the center of bearing 28. Further, tapered second baseplate outwardly facing aperture wall surface 76 is tapered to a larger diameter toward the second baseplate outwardly facing surface 26. Additionally, and preferably, the conformation of the taper matches the contour defined by second retaining cap inwardly facing tapered surface 80. Since second retaining cap 34 and compression locking post 14 are stationary with respect to bearing 28, such tapering and conformation of tapered second baseplate outwardly facing aperture wall surface 76 permits second baseplate 30 to rotate (about the centroid of motion at the center of bearing 28) with respect to bearing 28 until the point at which second baseplate 30 interferes with, or contacts, the second retaining cap inwardly facing tapered surface 80. Therefore, the taper, diameter, and conformation of these interacting elements (i.e., the formation of the space between second retaining cap 34 and second baseplate 30) can be established to limit the rotational ability of the second baseplate 30 relative to bearing 28. Preferably, the taper, diameter, and conformation of these interacting elements accommodate rotation of second baseplate 30 relative to bearing 28 at least until baseplate inwardly facing surfaces 20, 24 of baseplates 10, 30 meet. In other words, the ability of second baseplate 30 to rotate relative to bearing 28 is limited by the distance between second retaining cap inwardly facing tapered surface 80 and second baseplate 30, as well as the distance between baseplates 10, 30.

[0054] In the preferred embodiment of the present invention, the axial rotation of baseplates 10, 30 (about the longitudinal axis of the spine) is unlimited. In other embodiments, the axial rotation is limited, preferably to from 7 to 10 degrees. This limitation may be created using a variety of methods including, for example, a notch formed in retaining caps 12, 34 and a groove formed in baseplates 10, 30. Alternatively,

the groove may be formed in retaining caps 12, 34 and the notch may be formed in baseplates 10, 30.

[0055] As best shown in FIGS. 1g and 1h, clearance exists between the baseplates 10, 30 and the bearing 28, as well as between the baseplates 10, 30 and the retaining caps 12, 34, whereby the baseplates 10, 30 are not only capable of rotating and angulating about the centroid of motion at the center of the bearing 28, but also capable of floating along the axial direction relative to each other, thus realizing a universal motion of the baseplates. When the baseplates float toward each other, the retaining caps 12 and 34 may protrude slightly beyond the outwardly facing surfaces of the baseplates 10, 30, and are accepted by the spaces formed by the concave contour of the endplates of the vertebral bodies.

[0056] The diameter of bearing 28, and its corresponding ability to withstand compression and tension stress loads, can be increased without a need to increase the height of the bearing 28 (which is limited by the spacing between adjacent vertebral bodies). Increasing the diameter of bearing 28 also increases the bearing surface and reduces point loading. Consequently, a more robust artificial intervertebral disc is achieved that is capable of withstanding the naturally occurring compression and tension forces exerted by adjacent vertebral bodies.

[0057] Whereas specific embodiments of an artificial intervertebral disc have been described and illustrated herein, it will be apparent to those of skill in the art that variations and modifications to that disclosed herein are possible without deviating from the broad spirit, scope, and principles of the present invention. Therefore, the present invention shall not be limited to the specific embodiments disclosed herein.